



Clinical applications of resting state functional connectivity

Michael D. Fox^{1*} and Michael Greicius²

¹ Partners Neurology Residency, Massachusetts General Hospital, Brigham and Women's Hospital, Harvard Medical School, Boston, MA, USA

² Department of Neurology and Neurological Sciences, Stanford University School of Medicine, Stanford, CA, USA

Edited by:

Lucina Q. Uddin,
Stanford University, USA

Reviewed by:

F. Castellanos,
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*Correspondence:

Michael D. Fox,
Partners Neurology Residency,
Massachusetts General Hospital,
Brigham and Women's Hospital,
Harvard Medical School, 55 Fruit St.,
Boston, MA 02114, USA.
e-mail: foxmdphd@gmail.com

During resting conditions the brain remains functionally and metabolically active. One manifestation of this activity that has become an important research tool is spontaneous fluctuations in the blood oxygen level-dependent (BOLD) signal of functional magnetic resonance imaging (fMRI). The identification of correlation patterns in these spontaneous fluctuations has been termed resting state functional connectivity (fcMRI) and has the potential to greatly increase the translation of fMRI into clinical care. In this article we review the advantages of the resting state signal for clinical applications including detailed discussion of signal to noise considerations. We include guidelines for performing resting state research on clinical populations, outline the different areas for clinical application, and identify important barriers to be addressed to facilitate the translation of resting state fcMRI into the clinical realm.

Keywords: fMRI, fcMRI, neurological disease, psychiatric disease, brain, spontaneous activity, intrinsic activity

INTRODUCTION

Functional magnetic resonance imaging (fMRI) is a non-invasive technique for examining brain function that utilizes changes in blood oxygen level-dependent (BOLD) signal to identify areas of increased or decreased neuronal activity (Logothetis, 2003; Raichle and Mintun, 2006). This technique has proven extremely valuable in the laboratory environment, allowing researchers to identify brain areas associated with the processing of different stimuli or the performance of various cognitive tasks (Raichle, 2000). Further, fMRI has been used extensively to identify abnormalities in these activation patterns in populations of patients with neurological or psychiatric disease.

Despite its success and popularity as a research tool, fMRI has seen relatively little translation into the clinical realm. In general, the fMRI abnormalities seen in clinical research populations have not translated into the ability to obtain useful diagnostic or prognostic information in individual patients (Matthews et al., 2006). While pre-operative fMRI is being used in individual patients to guide neurosurgical intervention, its use has not yet been shown to improve patient outcomes. Although progress is certainly being made, the clinical utility of fMRI has yet to be firmly established.

A recent advance that offers tremendous promise for improving the clinical applicability of fMRI involves focusing on spontaneous modulations in the BOLD signal that occur during resting conditions (for recent review see Fox and Raichle, 2007). In contrast to the traditional task-based approach, resting state studies observe the brain in the absence of overt task performance or stimulation. In these studies, subjects are generally asked to lie quietly under "resting" conditions such as eyes closed or while fixating on a crosshair. Spontaneous modulations in the BOLD signal in the absence of any explicit input or output are then recorded and analyzed. Although alternative approaches exist (Zhu et al., 2005,

2008; Cao et al., 2006; Fox and Raichle, 2007; Zang et al., 2007; Biswal et al., 2010), analysis of these spontaneous fluctuations usually involves the identification of correlations between remote brain areas, commonly referred to as functional connectivity. The term "functional connectivity" has been used in both resting-state and task-state studies and can refer to correlations across subjects, runs, blocks, trials, or individual BOLD time points, an ambiguity which can become confusing (Friston et al., 1993; Horwitz, 2003; Fox and Raichle, 2007; Rogers et al., 2007). We will therefore use the term resting state functional connectivity MRI (fcMRI) for added specificity, and this will be the focus of the present article. The two most popular techniques for performing resting state fcMRI are seed-based correlations and independent components analysis (ICA). In the seed-based technique signal is extracted from a specific region of interest, and a map is created by computing the correlation between this extracted signal and all other brain voxels (Biswal et al., 1995; Fox and Raichle, 2007). In contrast, ICA considers all voxels at once and uses a mathematical algorithm to separate a dataset into distinct systems or networks that are correlated in their spontaneous fluctuations but also maximally independent, usually in the spatial domain (Kiviniemi et al., 2003; Bartels and Zeki, 2004; Beckmann et al., 2005).

Regardless of the technique, a consistent observation is that regions with similar functional properties, such as the left and right somatomotor cortices, exhibit coherent BOLD fluctuations even in the absence of movement under resting conditions (Biswal et al., 1995; Lowe et al., 1998; Cordes et al., 2000; De Luca et al., 2005; Fox et al., 2006b). Similar results have been found in multiple other networks including visual (Lowe et al., 1998; Cordes et al., 2000), auditory (Cordes et al., 2000), language (Cordes et al., 2000; Hampson et al., 2002), dorsal and ventral attention systems (Fox et al., 2006a), corticothalamic circuits (Zhang et al., 2008), and a frontal opercular network that has been related to stimulus salience

(Seeley et al., 2007b). One of the most robustly identified and extensively investigated resting state networks involves a set of regions that routinely decrease their activity during attention demanding tasks, often referred to as the default mode network (Raichle et al., 2001; Greicius et al., 2003; Fox et al., 2005; Fransson, 2005) (Figure 1). Interestingly, this network has also been found to be negatively or anti-correlated with regions that tend to increase their activity during attention demanding tasks (Greicius et al., 2003; Fox et al., 2005, 2009; Fransson, 2005; Chang and Glover, 2010). Resting state correlation patterns across various networks have been shown to predict the task-response properties of brain regions (De Luca et al., 2005; Vincent et al., 2006), identify subjects' aptitude for different cognitive tasks (Hampson et al., 2006; Seeley et al., 2007b), and help constrain and refine neuro-anatomical models developed on the basis of task-activation studies (Fox et al., 2006a; Dosenbach et al., 2007).

Given the success of resting state functional connectivity for probing the brain's functional architecture in normal subjects, it is only natural to apply the technique towards understanding brain disease. Two recent reviews detail the large number of studies that have utilized resting state fcMRI to study various neurological and psychiatric conditions (Greicius, 2008; Zhang and Raichle, 2010). Although this list continues to grow on a daily basis, the goal of the present article is not to review the findings from each individual study and the insight each provides towards understanding specific diseases. The field has expanded to the point that resting state reviews focused on each specific disease are rapidly becoming appropriate. Instead, we take a more global perspective on the application of resting state fcMRI in the clinical realm. We detail the theoretical and practical motivations for using resting state fcMRI for clinical applications, describe the different types of clinical applications to

which resting state may be applied, provide guidelines for using resting state fcMRI as a clinical tool, and identify barriers to full translation of resting state fcMRI into the clinical realm.

WHY USE RESTING STATE fcMRI FOR CLINICAL APPLICATIONS?

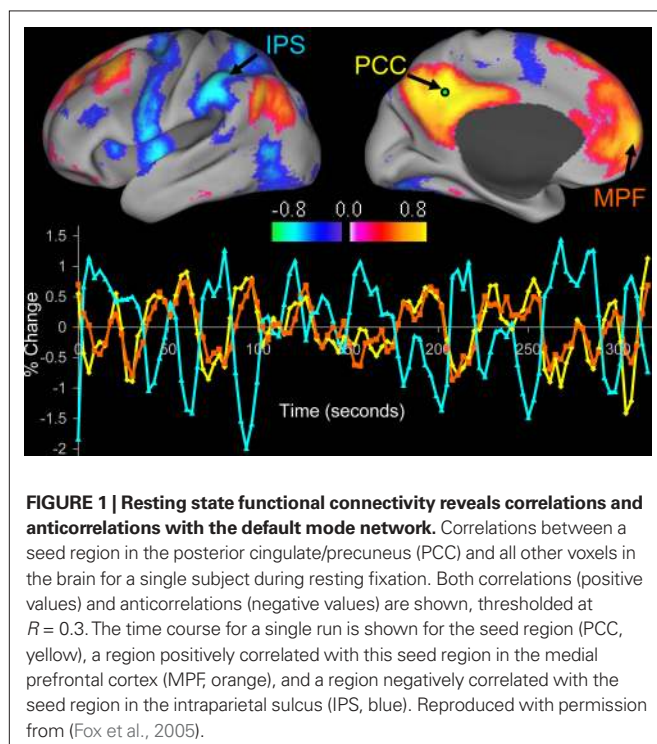
CEREBRAL ENERGETICS

There are several motivations, both theoretical and practical for using resting state fcMRI for clinical applications. The first of these motivations comes from an understanding of brain energy metabolism. The resting human brain represents only 2% of total body mass but consumes 20% of the body's energy, most of which is used to support of ongoing neuronal signaling (Ames, 2000; Attwell and Laughlin, 2001; Lennie, 2003; Shulman et al., 2004; Raichle and Mintun, 2006). Task-related increases in neuronal metabolism are usually small (<5%) when compared to this large resting energy consumption (Raichle and Mintun, 2006). Differences in these task-related changes between normal and pathological populations are smaller still, often less than 1%. When attempting to study disease or diagnose patients based on task-related changes, one is therefore focusing on only a very small fraction of the brain's overall activity. Ongoing spontaneous activity may provide a window onto the neural processing that appears to consume the vast majority of the brain's resources and so may prove a richer source of disease-related signal changes.

SIGNAL TO NOISE

Resting state studies may offer a better signal to noise ratio than conventional task-based approaches. To demonstrate this principle, BOLD modulations recorded from the somatomotor cortex are shown during a simple task in which subjects were asked to press a button with their right hand (Figure 2) (Fox et al., 2006b). In this case, the subject pressed the button only once during the scanning session. Examining the tracing from the left somatomotor cortex alone (Figure 2A), it is impossible to identify when during the session that button press occurred. The signal, or task-related modulation, is very small relative to the tremendous amount of ongoing noise. Even if one focuses only on the time of the button press itself, when task-related BOLD modulation is maximal, the task-related modulation accounts for only 20% of the total BOLD variance (Fox et al., 2006b, 2007b). This means that during a standard fMRI task session over 80% of the BOLD modulation may be discarded as noise. This is why task-related BOLD studies require a large number of trials and extensive averaging to obtain a signal or activation map, and this may be part of the reason why task-based fMRI has found only limited application in the clinical realm.

A critical observation that forms the basis of resting state fcMRI was the finding that much of this "noise" that is so problematic for task-based studies is actually ongoing spontaneous fluctuations that are correlated within distinct cortical networks. This becomes apparent in our button press example when one adds the tracing from the right somatomotor cortex, which is only minimally involved in the right-handed task, to the tracing already shown for the left somatomotor cortex (Figure 2B). Much of the "noise" in the left somatomotor cortex is also present on the right. It is important to note that this shared variance is specific



to the somatomotor system and can be directly tied to variability in motor function (Fox et al., 2006b, 2007b). Even if one focuses only on the button press epoch, spontaneous ongoing activity can account for around 60% of the BOLD “noise” (Fox et al., 2006b, 2007b). In fact, one can subtract the ongoing spontaneous activity from the left somatomotor cortex and the single button press response becomes evident (Figure 2C).

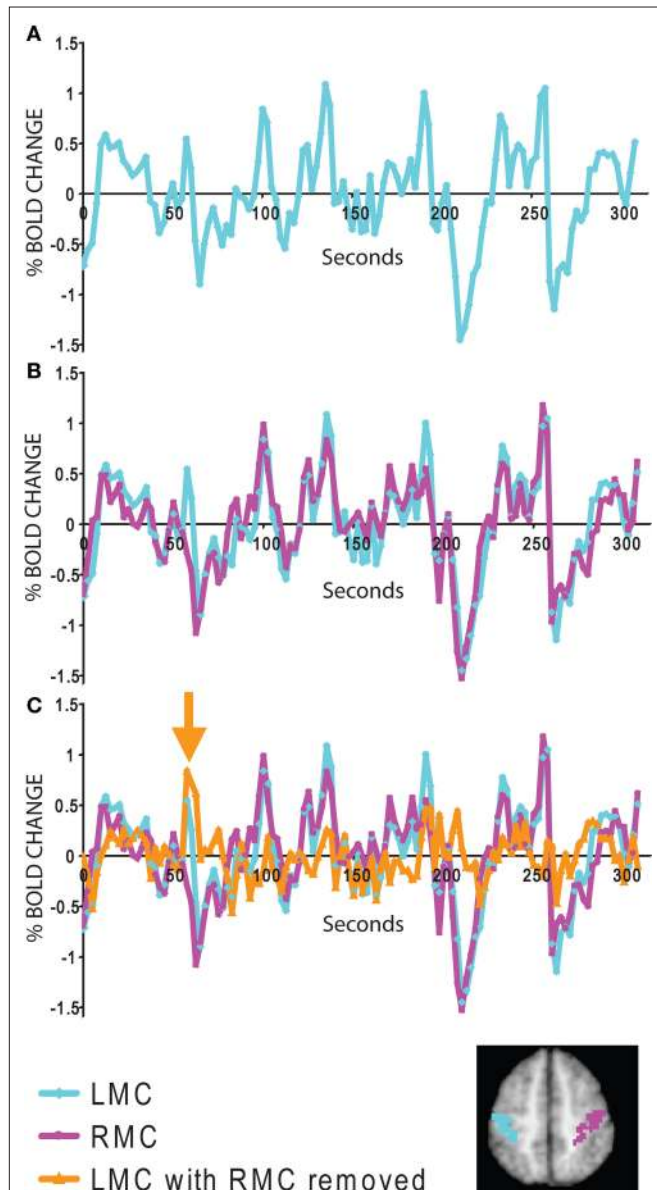


FIGURE 2 | Signal to noise features of spontaneous and task evoked activity. (A) fMRI time course from the left somatomotor cortex (LMC) during a single run when the subject pressed the button once with his right hand. Due to poor signal to noise, it is impossible to identify the task-related activity. **(B)** Comparison of the LMC with the right somatomotor cortex (RMC) shows that much of the noise is ongoing spontaneous activity correlated within the somatomotor system. **(C)** After subtracting the RMC from the LMC, the task-related modulation from the individual button press is evident (orange arrow). The LMC and RMC regions of interest are displayed for convenience on the inset map. Data taken from (Fox et al., 2006b).

Task-activation studies have a poor signal to noise ratio because the signal (task-related modulation) is often small relative to the sea of ongoing noise (including spontaneous activity). In contrast, resting state fcMRI focuses on this ongoing spontaneous activity and uses it as the signal rather than discarding it as noise. System-specific correlation values can be as high as 0.7–0.9 (accounting for 50–80% of the variance) (Fox et al., 2006b, 2007b) (see Figure 1). Compared to the 20% signal to noise ratio seen in task-based activation studies, resting state fcMRI studies may enjoy approximately three times the signal to noise ratio. Although additional signal to noise considerations exist (see final section), a 3 to 1 improvement in signal to noise has obvious advantages when attempting to identify imaging abnormalities in individual patients.

MULTI-PURPOSE DATA SETS

In addition to the above signal to noise considerations, resting state fcMRI data sets can be used to study multiple cortical systems. This is in contrast to task-activation analyses which require dedicated data acquisitions for each function one is attempting to localize. For example, if one wants to identify both motor and language systems for pre-operative mapping one would need to perform one acquisition of a motor task and another acquisition of a language task. In fcMRI the same data can be used to examine both systems, effectively doubling the amount of data (or alternatively reducing the acquisition time by half).

EXPANDED PATIENT POPULATIONS

One of the most frequently cited motivations for using resting state fcMRI in clinical studies is that it allows for a broader sampling of patient populations. Due to cognitive dysfunction or physical impairment many patients are simply not capable of performing tasks accurately in the fMRI scanner. When studying disease, this often means that we are sampling the least impaired subjects in a patient group as opposed to the most impaired subjects likely to show the largest signal abnormalities. In addition to limiting our sensitivity for detecting disease related changes, this introduces the problem of whether observed abnormalities can be generalized to the average (and often sicker) disease population. Resting state fcMRI requires no task and places only minimal demands on the patient. Further, spontaneous activity continues when subjects are asleep (Fukunaga et al., 2006; Horovitz et al., 2006) and sedated (Kiviniemi et al., 2003; Peltier et al., 2005; Vincent et al., 2007; Greicius et al., 2008b) opening up the possibility of obtaining resting state activity in any patient population. Of note, it remains unclear if individual differences observed during the awake state persist during sleep or sedation and is an important area for future research.

CIRCUMVENTING TASK-RELATED CONFOUNDS

One important advantage of resting state fcMRI is that it may circumvent confounds that can complicate interpretation of task-based studies. For example, working memory tasks have been used extensively to study patients with schizophrenia. However, a difference in activation between patients and control subjects observed during the task could represent differences in task performance, effort, task strategy, or an underlying disease-specific brain abnormality. A second example involves longitudinal studies

which utilize repeated task-based scanning sessions to examine drug effects or disease progression. These repeated task sessions can be confounded by practice effects or adaptation to the task. By eliminating the task, resting state fcMRI can circumvent some of these interpretative ambiguities and may allow for identification of more fundamental abnormalities underlying disease.

TYPES OF CLINICAL APPLICATIONS

IDENTIFYING GROUP DIFFERENCES IN BRAIN DISEASE

Although there are several ways in which resting state fcMRI may be applied to clinical populations, by far the largest application has been comparing resting state correlation patterns between groups of normal subjects and those with neurological or psychiatric disease (for recent reviews see Fox and Raichle, 2007; Greicius, 2008; Zhang and Raichle, 2010). The goal is that through identification of group differences one may begin to better understand the functional abnormalities underlying different disease states leading ultimately to a reliable resting state fcMRI marker that can be interpreted at the single subject level. This knowledge could in turn lead to identification of new treatments or drug targets. Disturbances in the correlation structure of spontaneous activity have now been reported for a significant number of disease states (see Table 1).

The goal of the current review is not to detail the individual findings of over 60 publications across 20 disease states. As mentioned in the introduction, we are rapidly approaching the point where reviews of resting state abnormalities for each particular disease state are becoming appropriate. However, tabulating the studies in this manner does lead to a few important observations. First, resting state fcMRI studies have been published on almost all major neurological and psychiatric diseases as well as a number of related conditions. While replication plays a role, the novelty of simply comparing correlation patterns between two groups is subsiding, and the route is paved for more advanced analyses (see next section). Second, the consistency of resting state abnormalities varies greatly by disease state, from excellent consistency across Alzheimer's, MCI, and PIB-positive patients to inconsistent and occasionally opposing findings in schizophrenia. There may be several reasons for this heterogeneity, and some mechanism to reconcile disparate findings is needed. Third, a seemingly disproportionate number of studies seem to focus on the default mode network as opposed to other resting state networks. While this may be appropriate in diseases like Alzheimer's with known or theoretical pathology in these regions, some of this focus may stem from a misconception that the default mode network is somehow special in showing large-amplitude coherent BOLD fluctuations at rest (for additional discussion see Fox and Raichle, 2007; Zhang and Raichle, 2010).

OBTAINING DIAGNOSTIC AND PROGNOSTIC INFORMATION

Given the substantial group comparison literature now available (Table 1), the route is paved for more advanced analyses of resting state abnormalities. One important advance is to relate the resting state differences seen between two groups to a relevant clinical variable. For example, pathological disturbances in intrinsic activity have been correlated with the severity of disease in depression (Greicius et al., 2007), schizophrenia (Bluhm et al., 2007), and neglect (He et al., 2007). Relating resting state

abnormalities to a relevant clinical variable speaks directly to the potential clinical relevance of a given finding and greatly increases confidence that the reported resting state abnormality will be reproducible.

Another important advance towards identifying prognostic or diagnostic markers on individual patients is to calculate the ability of observed resting state abnormalities to segregate healthy from disease states. Not surprisingly, the vast majority of this work has focused on the disease state with the most reproducible resting state abnormalities, Alzheimers, (Li et al., 2002; Greicius et al., 2004; Wang et al., 2006a; Supekar et al., 2008) (Figure 3) and the potentially associated condition of PIB positivity (Hedden et al., 2009; Sheline et al., 2010). By looking at different resting state fcMRI measures and setting a threshold, one can calculate the sensitivity and specificity of that marker for segregating healthy and disease states (Figure 3A). In Alzheimers, sensitivity ranges from 72–85% and specificity from 77–80% (Li et al., 2002; Greicius et al., 2004; Wang et al., 2006a; Supekar et al., 2008). Instead of picking just one threshold, receiver operating characteristic (ROC) curves can show the sensitivity and specificity at several different thresholds and have been usefully applied in Alzheimers (Li et al., 2002; Supekar et al., 2008) (Figures 3B,C). Although not yet applied to Alzheimers, techniques such as machine vector learning and advanced pattern recognition may further improve the utility of resting state fcMRI abnormalities as brain disease biomarkers (Haynes and Rees, 2006; Norman et al., 2006). Thus far, these segregation studies have been retrospective and the criteria for identifying a disease has been optimized for a specific data set. Future work applying these criteria prospectively towards new datasets will serve as an important test of their potential clinical relevance as a diagnostic or prognostic marker.

LONGITUDINAL STUDIES AND TREATMENT EFFECTS

One area for which resting state fcMRI is extremely well suited is longitudinal studies and monitoring treatment effects. For example, much may be learned by following disease progression in neuro-degenerative disorders such as Alzheimer's or amyotrophic lateral sclerosis (ALS). Similarly, one can examine the effect of clinical intervention by studying subjects before and after treatment. Normalization of resting state brain abnormalities with drug therapy may prove to be a useful surrogate outcome in clinical trials or help pharmaceutical companies decide which drugs to bring to large-scale clinical trials in the first place. Along these lines, resting state fcMRI abnormalities in depression have been shown to dissipate with drug treatment (Anand et al., 2005b), and improvement in regional correlations has been shown to match functional recovery in spatial neglect following stroke (He et al., 2007).

CLUSTERING IN HETEROGENEOUS DISEASE STATES

To date segregation has focused largely on differentiating healthy from disease states. However one important role for resting state connectivity analyses may be segregating patients within a disease category. For example, schizophrenia is widely regarded as a very heterogeneous disorder, and this heterogeneity can greatly hinder the sensitivity of clinical trials. One could imagine placing the resting state patterns of hundreds of patients with schizophrenia into an algorithm that would cluster the patients into groups

Table 1 | Group differences in resting state fcMRI patterns observed in various brain diseases or conditions.

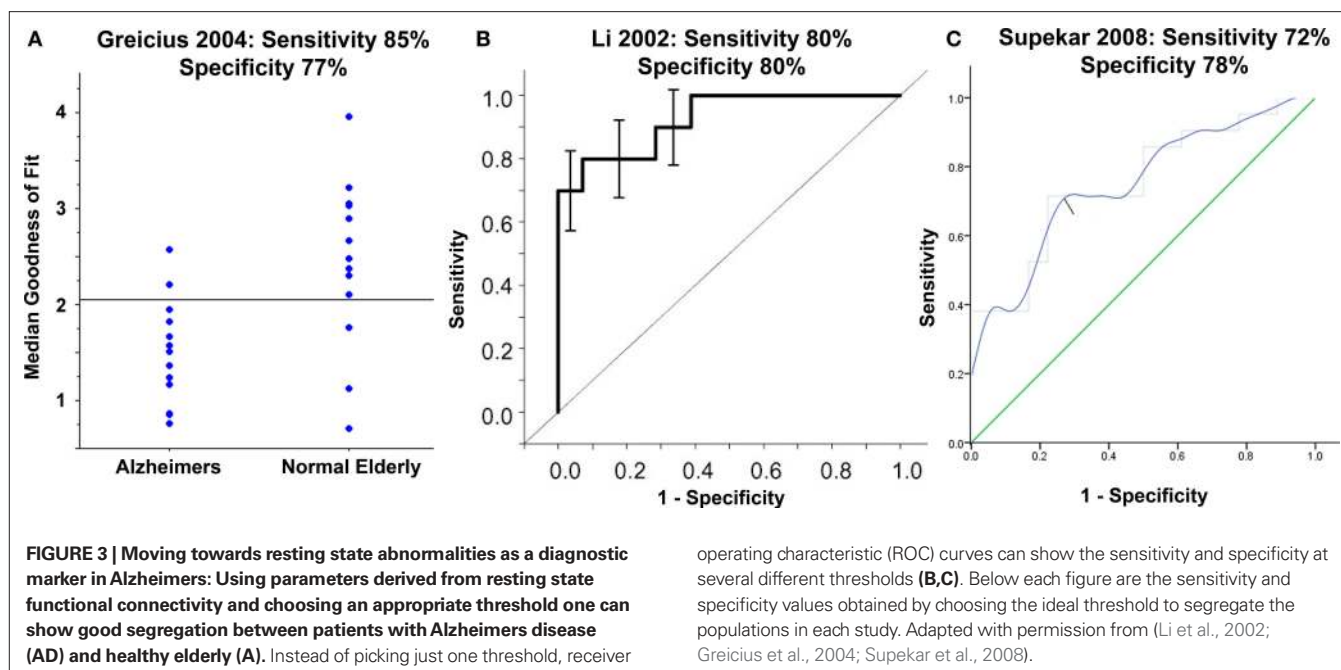
Disease/condition	References	Findings
Alzheimer's	(Li et al., 2002; Greicius et al., 2004; Wang et al., 2006a,b, 2007; Allen et al., 2007; Supekar et al., 2008)	Decreased correlations within the DMN including hippocampi, decreased anticorrelations with the DMN, and reduced local connectivity as reflected in clustering coefficients
PIB positive	(Hedden et al., 2009; Sheline et al., 2010)	Decreased correlations within the DMN
Mild cognitive impairment	(Li et al., 2002; Sorg et al., 2007)	Decreased correlations within the DMN and decreased anticorrelations with the DMN.
Fronto-temporal dementia	(Seeley et al., 2007a, 2008)	Decreased correlations within the salience network
Healthy aging	(Andrews-Hanna et al., 2007; Damoiseaux et al., 2008)	Decreased correlations within the DMN
Multiple sclerosis	(Lowe et al., 2002; De Luca et al., 2005)	Decreased correlations within the somatomotor network
ALS	(Mohammadi et al., 2009)	Decreased connectivity within the DMN and within the somatomotor network (esp. premotor cortex)
Depression	(Anand et al., 2005a,b, 2009; Greicius et al., 2007; Bluhm et al., 2009a)	Variable: Decreased corticolimbic connectivity (esp. with dorsal anterior cingulate), increased connectivity within the DMN (esp. subgenual prefrontal cortex), decreased connectivity between DMN and caudate
Bipolar	(Anand et al., 2009)	Decreased corticolimbic connectivity
PTSD	(Bluhm et al., 2009c)	Decreased connectivity within the DMN
Schizophrenia	(Liang et al., 2006; Liu et al., 2006, 2008; Bluhm et al., 2007, 2009b; Salvador et al., 2007; Zhou et al., 2007; Jafri et al., 2008; Whitfield-Gabrieli et al., 2009)	Variable: Decreased or increased correlations within the DMN. Decreased, increased or unchanged correlations and anticorrelations between the DMN and other systems.
Schizophrenia 1° relatives	(Whitfield-Gabrieli et al., 2009)	Increased connectivity within the DMN
ADHD	(Zhu et al., 2005, 2008; Cao et al., 2006; Tian et al., 2006; Zang et al., 2007; Castellanos et al., 2008; Wang et al., 2009)	Variable: reduced connectivity within the DMN, reduced anticorrelations with the DMN, increased connectivity in the salience network
Autism	(Cherkassky et al., 2006; Kennedy and Courchesne, 2008; Monk et al., 2009; Weng et al., 2010)	Decreased connectivity within the DMN (although hippocampus is variable and connectivity may be increased in younger patients)
Tourette syndrome	(Church et al., 2009)	Delayed maturation of task-control and cingulo-opercular networks
Epilepsy	(Waites et al., 2006; Lui et al., 2008; Bettus et al., 2009; Zhang et al., 2009b,c)	Variable: decreased connectivity in multiple networks including the medial temporal lobe, decreased connectivity within the DMN (esp. in patients with generalized seizures)
Blindness	(Liu et al., 2007; Yu et al., 2008)	Decreased connectivity within the visual cortices and between visual cortices and other sensory and multimodal regions
Chronic pain	(Greicius et al., 2008a; Cauda et al., 2009a,c,d)	Variable: Increased/decreased connectivity within the salience network, decreased connectivity in attention networks
Neglect	(He et al., 2007)	Decreased connectivity within the dorsal and ventral attention networks
Coma/vegetative state	(Boly et al., 2009; Cauda et al., 2009b; Vanhaudenhuyse et al., 2010)	Progressively decreased DMN connectivity with progressive states of impaired consciousness
Generalized anxiety disorder	(Etkin et al., 2009)	increased connectivity between amygdala and frontoparietal control network and decreased connectivity between amygdala and salience network

DMN = default mode network including regions in the posterior cingulate/precuneus, lateral parietal cortex, medial temporal lobes, and medial prefrontal cortex (see Figure 1). Salience network: includes regions in the dorsal anterior cingulate and bilateral fronto/insular cortices; dACC = dorsal anterior cingulate cortex; PIB = Pittsburgh compound B, a marker of amyloid plaque accumulation in the brain. PTSD = post-traumatic stress disorder; ALS = amyotrophic lateral sclerosis; ADHD = attention deficit hyperactivity disorder. Note: some references (Greicius et al., 2004; He et al., 2007) reflect "near-rest" conditions in which task-related variance has been minimized and other references (Zhu et al., 2005, 2008; Cao et al., 2006; Zang et al., 2007) reflect local changes in spontaneous BOLD fluctuations as opposed to correlations in these fluctuations between separate regions.

with similar resting state abnormalities. Similarly, retrospective analysis of drug effects could identify subgroups that benefited from a particular therapy.

PRE-OPERATIVE MAPPING AND TARGETING INTERVENTION

The area in which traditional task-based fMRI has shown the greatest promise for clinical translation is in pre-operative functional



brain mapping to help guide neurosurgical planning (Haberg et al., 2004; Vlieger et al., 2004; Matthews et al., 2006). This is used most often to identify brain areas used in movement and language so that these areas can be avoided during surgical resection, but it has also been combined with EEG to identify foci of epileptic activity (Lemieux, 2004). fMRI defined brain regions correlate with intra-operative electrophysiology (Vlieger et al., 2004), Wada testing (Binder et al., 1996; Adcock et al., 2003), loss-of-function post-operatively (Haberg et al., 2004), and are frequently mentioned in neurosurgery notes (Haberg et al., 2004). However, patients frequently lack the ability to perform tasks well (Pujol et al., 1998) and patient movement during tasks can be a significant problem (Lee et al., 1999).

As mentioned earlier, the advantages of resting state fMRI may circumvent many of the current limitations hindering task-based pre-operative mapping. Indeed several articles have recently been published showing strong proof of concept for resting state fcMRI as a pre-operative mapping tool in patients with neurosurgical conditions (Kokkonen et al., 2009; Liu et al., 2009; Shimony et al., 2009; Zhang et al., 2009a). These articles have shown good correlation between resting state fcMRI results, task-based mapping, and intra-operative cortical stimulation in these patients (Figure 4).

Just as resting state fcMRI may guide surgeons in their operative approach, it may also be used to guide several other clinical interventions where localization of a functional region is critical. Examples include placement of EEG recording grids, deep brain stimulators, and transcranial magnetic stimulation (TMS).

BARRIERS TO CLINICAL APPLICABILITY/FUTURE WORK

GUIDELINES FOR STUDYING CLINICAL POPULATIONS WITH fcMRI

Despite the promise of resting state fcMRI for improving the translation of functional imaging into the clinical realm, several challenges remain. One of the largest barriers is inconsistent

Table 2 | Guidelines for studies of clinical populations with resting state fcMRI.

- (1) *A priori* hypotheses regarding a region or network with abnormal fcMRI and clear criteria for selecting this region or network
- (2) *A priori* hypothesis and demonstration of a region or network with normal fcMRI to serve as a control
- (3) Correlation with clinical variables whenever possible
- (4) Stringent correction for multiple comparisons
- (5) An analysis of movement in patients and control subjects
- (6) An analysis of the differential impact of pre-processing in patients and control subjects
- (7) A discussion of how current findings relate to prior fcMRI findings

results across studies. When studies are relatively consistent, as in Alzheimers, it is easy to build on these results and move towards using resting state fcMRI for diagnostic and prognostic purposes. However, when studies are inconsistent as in schizophrenia, one is left wondering which result, if any, is most likely to be reproducible and therefore clinically relevant. Different study designs, processing techniques, analysis approaches, and regions or systems of interest make comparing studies very difficult.

One of the first steps towards improving translation is to begin to improve our ability to replicate and compare results from different resting state studies. While individual labs will always differ in their analytical approach (and this is a good thing) there are certain standards or guidelines that may help improve reproducibility and strengthen the conclusions that can be made (Table 2). Some of these guidelines may appear generic and obvious, however resting state fcMRI presents a unique set of challenges in study design and analysis that may benefit from explicit delineation.

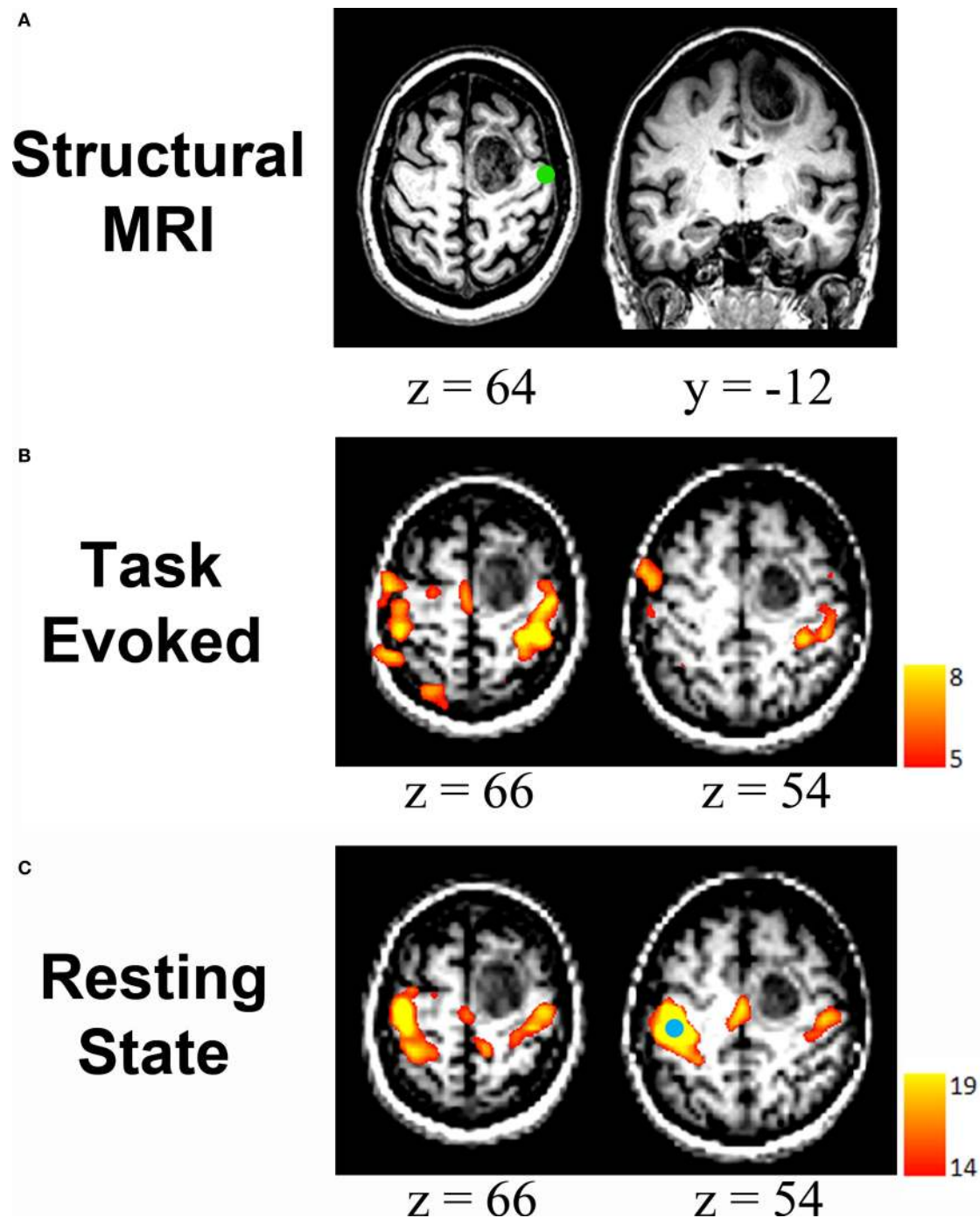


FIGURE 4 | Resting state fcMRI in pre-operative brain mapping:

(A) Structural MRI scan showing a mass in the right frontal cortex. Green circle represents the location of ipsilateral hand response to intra-operative cortical stimulation. (B) Task-related mapping showing activity within the sensorimotor network but also small responses in parietal cortex that are seemingly

unrelated to motor function or sensation. (C) Resting-state correlation mapping showing that the sensorimotor network is largely unaffected by the tumor anterior to the central sulcus. Seed region is shown (blue circle). All images are displayed left-on-left. Adapted with permission from (Zhang et al., 2009a).

(1) The first guideline concerns a priori identification of either a region (seed-based analysis) or network (ICA) that one expects may be abnormal. This hypothesis can be based on prior imaging data (either task-based or resting state), pathology, or simply the clinical features of the disease combined

with theory suggesting localization of the relevant impaired functions. If the a priori motivation for the study is clearly presented in the introduction, then even a well-powered, negative finding can represent an advance. Analyses of a large number of seed regions or components can be an effective

means of generating hypotheses, but such exploratory work must be followed by targeted analyses that are powered to disconfirm spurious findings. Similar to choosing which region or network one is interested in, one must also clearly identify a priori how that network will be identified. If one is using a seed region, the coordinates for that seed region should be justified, for example as a focus of activation from a previously published study. Similarly, if one is studying a network in the form of an ICA component, one needs to specify an objective approach for identifying that system such as spatial correlation to an a priori template (Greicius et al., 2004, 2007), however see also (Zuo et al., 2009) for possible limitations of this approach.

- (2) Perhaps as important as the first guideline, the second guideline involves a priori identification of regions or networks that one expects NOT to vary between the disease and healthy state. A good choice for many diseases may be primary sensory systems such as visual, somatomotor, or auditory. Of course, it is theoretically possible that a disease state exists which impacts every brain system and region such that a normal control is not possible. However in these cases alternative control strategies should be pursued to show that the findings are not artifactual.
- (3) As mentioned in an earlier section, any study which can show a relationship between identified resting state fcMRI abnormalities and clinical variables such as disease severity increases the confidence that a finding will be clinically relevant and reproducible.
- (4) The fourth guideline concerns correction for multiple comparisons. This becomes especially pertinent if one is looking for differences across a large number of seed regions or components or if one is attempting to correlate resting state abnormalities with several different clinical variables. The probability of finding a significant relationship increases as the number of variables one is trying to relate increases. Several methods to correct for these multiple comparisons exist, the simplest and most stringent being Bonferroni correction (Abdi, 2007). Clearly there are cases where one doesn't know a priori which clinical variable or component may be of interest, and an effect that does not pass Bonferroni does not mean the effect is not interesting, it simply means that the relationship would benefit from repeat and targeted testing.
- (5) The fifth guideline concerns movement correction and comes from the recognition that patient populations are often going to be less cooperative lying in the scanner than control populations, especially when they are required to do nothing but stare at a fixation cross for 10 min. While task-based studies can partially compensate for movement by averaging across a large number of trials, the nature of the signal used in resting state makes it particularly susceptible to movement confounds. Movement parameters are often used as co-regressors in resting state fMRI to try to minimize artificial correlations, however if large group differences in movement are present this remains a confounding variable. In such instances, one could look to see if movement correlated on a subject to subject basis with the finding of interest. If the patients that moved the most also showed the largest difference in resting state correlation values then there should be an elevated index of suspicion. Note that identification of control networks that are not different between the two groups will also help in this regard (see point #2).
- (6) Similar to the above movement analysis, one should examine the impact of pre-processing on the two groups of subjects to insure that they do not differ. For example, much has been written on the pronounced effect of global signal regression on resting state correlations and anticorrelations (Chang and Glover, 2009, 2010; Fox et al., 2009; Murphy et al., 2009; Weissenbacher et al., 2009). Although there is benefit to this pre-processing maneuver including improved correspondence with anatomical connectivity (Fox et al., 2009), one must ensure that the effect of the pre-processing was not different in the two groups. In this example, one could examine the variance removed by global regression and show that it is not significantly different between patients and controls. If there is a group difference then one may want to repeat the analysis without removing the global signal and determine if the effect of interest remains. Similarly in ICA, there is a large impact on results based on the number of components one chooses. Due to a difference in variance in a patient population from movement or any other confounding factor, a certain component could be split at a different point in patients and controls. Repeating a finding with a slightly higher or lower number of components (such as plus and minus 25% of the initial number of components) could increase confidence in the result.
- (7) The final guideline concerns reconciling findings with previously published work. Although this point may seem obvious and is certainly not specific to resting state fcMRI, its importance makes it worth mentioning. If the current resting state fcMRI findings conflict with prior fcMRI work, it is crucial to explore possible etiologies of the conflict. It should not be sufficient to simply mention that other work has been done with differing conclusions. Resolving the discrepancy may involve additional analyses to directly explore differences in processing methodology, but such analyses are critical for accelerating consensus in the field and clinical applicability.

THE CASE FOR COLLABORATION

Despite the increasing number of papers being published on a daily basis by individual labs, clinical applicability of fcMRI is not likely to move forward without enhanced collaboration and data sharing between labs. Different processing techniques for analyzing resting state data make comparison across studies difficult. The majority of resting state articles focus on a few seed regions or a single network, leaving unexplored the vast majority of the brain's functional architecture. Finally, almost all studies focus on normal subjects or a single disease population making it difficult to assess reproducibility or determine the sensitivity or specificity of an identified abnormality for a specific disease.

In this review we explored several factors that make resting state fcMRI well-suited for translation into the clinical realm. However there are also several features that make it well-suited for databasing, data sharing, and collaboration. Due to the nature of spontaneous BOLD data, a single dataset can be used for multiple analyses and can address a wide variety of neuroscience questions. Furthermore, the paradigms used to study spontaneous BOLD

activity are relatively simple compared to task-based imaging studies with multiple stimuli presented at varying intervals. These factors make spontaneous BOLD data ideally suited for reanalysis and inclusion in a database.

The above factors have motivated the creation of two online databases focused on resting state fMRI data. The first is both an analysis package and database termed BrainSCAPE (Spontaneous Correlation Analysis Processing Engine)¹ (Fox et al., 2007a). This tool allows users to upload, analyze, and share their spontaneous BOLD data as well as analyze freely shared data from other labs. More recently a second database has been launched termed the NITRIC 1000 connectome project² and includes a large number of functional connectivity datasets freely available for download (Biswal et al., 2010). By providing access to multiple datasets, effects in one study can easily be confirmed and compared with results from multiple other datasets. We anticipate that collaborative projects such as these will accelerate advances in the field and may prove valuable in assessing the sensitivity and specificity of intrinsic abnormalities underlying human disease.

TECHNIQUE DEVELOPMENT

Finally, an improvement in clinical utility is likely to come from further technique development. One area that is likely to be essential as we move from studies of groups of patients to obtaining prognostic and diagnostic information on a single patient is improving signal to noise. As mentioned at the beginning of this article, studies of resting state fluctuations do enjoy a potential signal to noise advantage over task-based studies. However, in task-based studies one can improve the signal to noise by simply increasing the number of trials and the amount of averaging. The technique for improving signal to noise in resting state studies is less straight forward. It is important to recognize that not all spontaneous BOLD fluctuations are due to underlying neuronal fluctuations in distinct cortical systems but may also come from non-neuronal sources. Although the quantitative impact of these noise sources is likely small relative to neuronal fluctuations, spontaneous BOLD modulation can be measured in a water phantom (Zarahn et al., 1997), and physiological fluctuations such as cardiac or respiratory activity can account for a significant fraction of spontaneous BOLD variance in human data (Glover et al., 2000; Wise et al., 2004; Birn et al., 2006; Lund et al., 2006; Chang and Glover, 2009). Improvements in signal to noise could therefore come from reducing the contribution of these non-neuronal fluctuations.

One strategy to account for non-neuronal noise is to employ a high sampling rate which prevents aliasing of higher frequency cardiac or respiratory activity (Biswal et al., 1995; Lowe et al., 1998; Cordes et al., 2001; De Luca et al., 2006); however this comes

with the limitation of reduced spatial coverage. Alternatively, physiological parameters can be measured during BOLD acquisition and removed from the data through linear regression (Glover et al., 2000; Rombouts et al., 2003; Birn et al., 2006; Deshpande et al., 2006; Lund et al., 2006; Chang et al., 2009; Chang and Glover, 2009). Finally, noise sources can be isolated from the BOLD data itself through techniques such as ICA (Kiviniemi et al., 2003; Bartels and Zeki, 2004; Beckmann et al., 2005), regressing out signals common to all voxels (the global signal) (Zarahn et al., 1997; Macey et al., 2004; Fox et al., 2005, 2009), or regressing out signals from regions likely to have a relatively high degree of physiological artifact relative to the amount of neuronal activity such as the ventricles or white matter (Rombouts et al., 2003; Fox et al., 2005). By improving signal to noise, one can begin to reduce scan time and improve clinical applicability.

Other technique advances that may be helpful are increasing the fMRI data that can be used for resting state analyses. For example, research may be expanded by using resting epochs from block design task data (Fair et al., 2007) or removing task-related variance and performing fMRI analyses on the residual (Arfanakis et al., 2000; Fair et al., 2007; He et al., 2007).

Finally, improved clinical applicability will likely come from moving beyond the fMRI scanner to multimodal investigations of spontaneous activity. Spontaneous fluctuations in the BOLD signal have been shown to correlate with EEG (Laufs et al., 2003), local field potentials (Shmuel and Leopold, 2008), and slow cortical potentials recorded with subdural electrode grids (He et al., 2008). Also resting state functional connectivity analyses are now being done with spontaneous fluctuations observed with near infrared spectroscopy (White et al., 2009). Such techniques raise the potential for studying continuous resting state correlations in situations where an MRI scanner is not practical such as real-time monitoring in intensive care units or operating rooms.

CONCLUSIONS

Resting state fluctuations in the BOLD signal of fMRI provide good signal to noise, require minimal patient compliance, can be obtained under anesthesia, and are well suited for translation into the clinical realm. Clinical applications include research studies focused on group differences, biomarkers for obtaining diagnostic and prognostic information in a single subject, and guidance of invasive and non-invasive treatments. Several guidelines for resting state studies of brain disease have been proposed here and may improve the reproducibility of findings and facilitate clinical translation. Finally, improvement in processing techniques of the fMRI signal as well moving beyond the fMRI signal to other modalities that can also assess low-frequency fluctuations are likely to be important as we begin to realize the potential of resting state fluctuations in the clinical realm.

¹www.brainscape.org

²www.nitrc.org/projects/fcon_1000

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